

## Review Article

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# Detection of metal ions in biological systems: A review

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**Abstract:** Metal ions are widely present in biological systems and participate in many critical biochemical processes such as material transportation, energy conversion, information transmission and metabolic regulation, making them indispensable substance in our body. They can cause health problems when deficiency or excess occurs. To understand various metabolic processes and facilitate diseases diagnosis, it is very important to measure the content and monitor the distribution of metal ions in individual cells, tissues and whole organisms. Among the various methods for metal ion detection, fluorescent sensors with organic dyes have attracted tremendous attention due to many advantages such as high fluorescence quantum yield, facile modification approaches and biocompatibility in addition to operation ease, high sensitivity, fast detection speed, and real-time detection. This review summarizes the recent progress on the detection and imaging of the metal ions in biological systems including  $\text{Na}^+$ ,  $\text{K}^+$ ,  $\text{Ca}^{2+}$ ,  $\text{Mg}^{2+}$ ,  $\text{Fe}^{2+}/\text{Fe}^{3+}$ ,  $\text{Zn}^{2+}$ , and  $\text{Cu}^{2+}$  provides an opinion on remaining challenges to be addressed in this field.

**Keywords:** metal ions sensing, fluorescent detection, fluorescent imaging, organic dyes

## 1 Introduction

Metal ions play crucial structural or functional roles in all life. They are required in essential biological processes such as osmotic regulation, catalysis, metabolism, and cell signaling. As the major metal ions in our body fluid, alkali metals ions,  $\text{Na}^+$  and  $\text{K}^+$  are responsible for maintenance of fluid and electrolyte balance, acid-base homeostasis, and maintenance of cell membrane potential allowing the generation of action potentials that are critical for neurotransmission, muscle contraction, and heart function [1]. Alkaline earth metal ions,  $\text{Ca}^{2+}$  and  $\text{Mg}^{2+}$ , play an important role in cell signaling including neurotransmission as well as their structural role and involvement in enzyme function [2,3]. Transition metals such as  $\text{Fe}^{2+}/\text{Fe}^{3+}$ ,  $\text{Zn}^{2+}$ ,  $\text{Cu}^{2+}$ , generally serving as a component of proteins and enzymes or activator of enzymes, are considered to be the critical players in many vital biological processes including oxygen transport, energy production, neurotransmission, regulation of gene expression and synthesis of essential molecules [4,5].

Although metal ions are critical for sustaining life, their concentration in organisms must be maintained within a proper range for optimal cellular function. Deficiency of these essential elements can cause serious health problems [6–8]. Excessive levels of these metal ions in our body or even extended exposure to them can also result in many health issues or toxicity [9,10]. Understanding the distribution and concentration fluctuation of metal ions in cells gives information on cell signaling, metabolic engineering and helps medical diagnosis. Thus, detection and imaging of metal ions in living organisms became a central topic in the bioanalytical and biomedical sciences. In the past decades, several spectrophotometric methods and electroanalytical techniques for metal ions detection have been developed, such as atomic absorption/emission spectroscopy [11,12], inductively coupled plasma mass spectroscopy (ICP-MS) [13,14], electrochemical assays [15,16], and colorimetric methods [17,18]. However, the application of these techniques is limited as they need expensive instrumentation and complicated pretreatments, which shows slow detection speed and does

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not permit the on-site instant detection and inspection of cells and living tissues. Fluorescent probes have become versatile tools due to their promising photophysical properties including high sensitivity and selectivity, low detection limit, fast response, operational simplicity, real-time monitoring and low cost [19,20]. Moreover, benefited from the new fluorescence imaging techniques, great progress has been made in the development of probes derived from organic fluorescent dyes (such as AIEgen, cyanine and rylene) [21–26] as they possess features such as good biocompatibility, high spatio-temporal resolution, facile chemical modification and they are capable of monitoring the subcellular localization and dynamics of biological targets [27–29]. This review summarized the recent advances of fluorescence sensing and imaging of metal ions in biological systems with the focus on probe design, responding mechanism and biological applications (Scheme 1).

Typical organic fluorescent probes are mainly composed of at least one fluorescent core and a metal chelating or binding moiety that recognizes different metal ions. There are several types of fluorescent cores such as rylencarboximide (RI), cyanine (Cy), rhodamine, difluoro-boron-dipyrromethene (BODIPY), etc. Upon metal binding, the electronic and/or molecular structure of the probes alters and it induces changes in fluorescence properties of the fluorophore, indicating the presence of metal ions. Fluorescent probes can be classified according to different criteria or characteristics. For instance, according to the responding mechanism, the probes can be divided into photoinduced electron transfer (PET) probes, fluorescence resonance energy transfer (FRET) probes, intramolecular charge transfer (ICT) probes, twisted intramolecular charge transfer (TICT) probes, through bond energy transfer (TBET) probes and aggregation-induced emission (AIE) probes. According to the optical performance, the probes can be divided into “off-on” probes, “on-off” probes and ratiometric probes. Fluorescent “off-on” probes and ratiometric probes

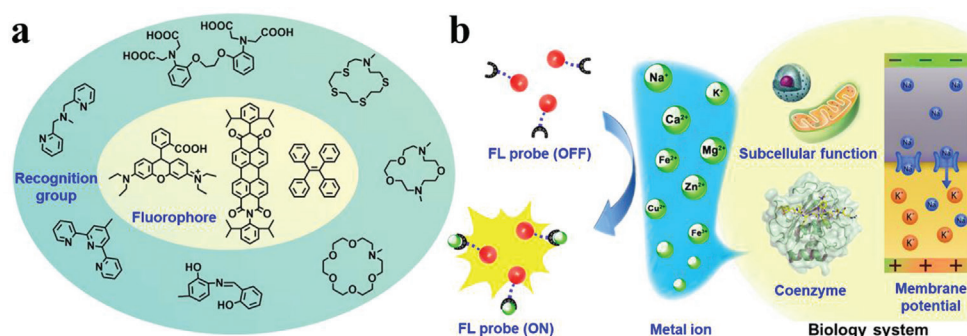
constitute the biggest group of fluorescent probes. The former features a fluorescent enhancement upon metal ions binding, the latter is based on the use of a ratio between two fluorescence intensities that allows correction of artifacts due to bleaching, changes in focus, and variations in laser intensity. Different types of fluorescent probes have been designed to adapt to various samples and systems, and can be used as powerful tools to study the function of metal ions in subcellular function, enzyme activity and dynamic change of membrane potential [30].

## 2 Detection of metal ions in biological systems

### 2.1 Probes for sodium ions ( $\text{Na}^+$ )

Sodium is the most abundant cation in extracellular fluid. It plays major roles in maintenance of fluid and electrolyte balance and regulates blood volume, blood pressure, osmotic equilibrium and pH values. The difference between the concentrations of sodium ions and potassium ions in extracellular and intracellular fluid causes the cell membrane potential which allows the cell to generate an action potential. Action potential is critical for body functions such as neurotransmission, muscle contraction, and heart function [31]. Absorption of sodium in the small intestine plays an important role in the absorption of chloride, amino acids, glucose, and water. Sodium is also an important component of gastric juice which aids the digestion and absorption of many nutrients. Therefore, the detection of  $\text{Na}^+$  ions is quite crucial for both clinical diagnosis and biochemical applications.

To achieve  $\text{Na}^+$  sensing and imaging in living cells, various types of fluorescent probes were developed. For instance, a DNzyme-based sensor was coupled with a catalytic hairpin assembly (to detect endogenous  $\text{Na}^+$



**Scheme 1:** Schematic illustration of the composition, (a) sensing mechanism and (b) biological applications of metal ions probe.

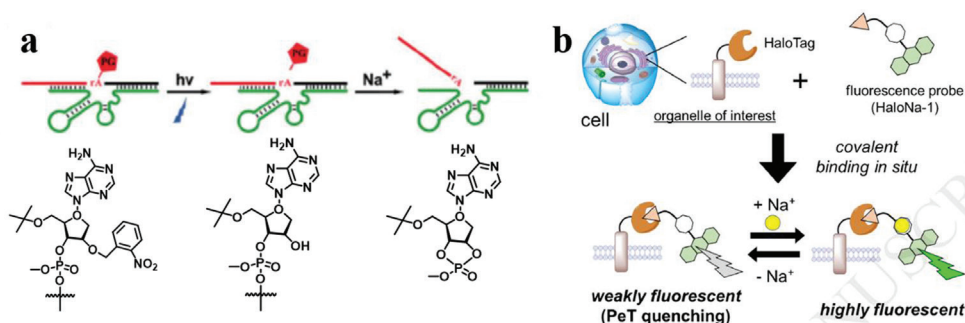
inside cells without the requirement for  $\text{Na}^+$  concentration increase by influx of the ions [32]. In their strategy, NaA43 DNazymes cleaved the substrate strands in the presence of  $\text{Na}^+$  and released initiator DNA that triggered the following CHA signal amplification reaction. In another case, a highly selective and robust  $\text{Na}^+$  aptamer was developed (Figure 1a). This probe contained two strands derived from the Ce13d DNzyme and a fluorescent adenine analog, 2-aminopurine (2AP) at the cleavage site of the substrate strand [33]. It was shown that the fluorescence was enhanced by  $\sim 40\%$  upon  $\text{Na}^+$  binding by introducing a 2AP at the cleavage site of the substrate strand and fluorescence quenching was observed upon  $\text{Na}^+$  binding by replacing a non-conserved adenine in the enzyme strand by 2AP. The fluorescence changes allowed for  $\text{Na}^+$  detection with a detection limit of 0.4 mM and signal saturation in less than 10 s. Apart from DNA based sensors, a protein-coupled  $\text{Na}^+$ -sensitive fluorescent probe, HaloNa-1, was developed [34] by conjugating a  $\text{Na}^+$  chelator, fluorescein, and a HaloTag ligand moiety (Figure 1b). The obtained probe could selectively label HaloTag-fusion proteins both *in vitro* and in cells, and its fluorescence was increased in response to concentration elevation of  $\text{Na}^+$ . Another fluorophore (mCherry) was introduced as an internal standard to eliminate signal artifacts. Two-photon fluorescence imaging with advantages such as minimized tissue autofluorescence background, a larger penetration depth, and reduced photodamage in biotissues has received enormous attention in both clinical diagnostics and basic biological research. Two-photon transition has strong excitation selectivity, which is conducive to imaging research on some special substances in biological tissues. Two-photon sensors were also prepared for the detection and imaging of  $\text{Na}^+$ . To achieve the quantification of  $\text{Na}^+$ , a fluorescent dye Asante NaTRIUM Green-2 (ANG-2) with  $\text{Na}^+$  sensitivity was reported and evaluated both *in vitro* and *in situ* with two-photon coupled fluorescence lifetime imaging microscopy [35].

It was found that the biexponential fluorescence decay behaviour of the dye *in situ* could be successfully analyzed in terms of quantitative  $[\text{Na}^+]$  recordings, indicating that ANG-2 is a promising new sodium indicator applicable for diverse biological systems. Moreover, two-photon microscopy was used for  $\text{Na}^+$  imaging to directly report the opening of voltage-gated sodium channels due to action potential propagation in mitral cells and the axonless granule cells [36].

## 2.2 Probes for potassium ions ( $\text{K}^+$ )

While sodium is the major cation outside animal cells, potassium is the major cation (positive ions) inside animal cells. Similar to sodium, potassium also has a major role in maintenance of fluid and electrolyte balance, acid-base homeostasis, systemic blood pressure control, hormone secretion and action, glucose and insulin metabolism and neurotransmission. Potassium deficiency and excess can each result in numerous signs and symptoms, including an abnormal heart rhythm and various electrocardiographic abnormalities. Highly selective and sensitive detection and imaging of physiological  $\text{K}^+$  is urgently needed for monitoring  $\text{K}^+$  related diseases and understanding the  $\text{K}^+$  involved physiological and pathological processes.

A TPE derivative modified DNA oligonucleotide fluorescent probe was reported for cellular  $\text{K}^+$  detection and imaging [37]. The probe exhibits  $\text{K}^+$  triggered AIE effect, and outstanding sensitivity with more extended photostability than most reported probes, and, thus, facilitates the long-lasting fluorescence imaging of  $\text{K}^+$  in living cells. To obtain probes with higher binding affinity to  $\text{K}^+$ , phenylaza-18-crown-6, a well-known ligand for  $\text{K}^+$  was adopted. Two molecular fluorescent probes based on the o-(2-methoxyethoxy) phenylaza-18-crown-6 lariat ether unit were reported [38]. These ratiometric fluorescent



**Figure 1:** (a) Synthesis of DNzyme-based  $\text{Na}^+$  probes. Reprinted with permission from reference [32]. (b) Probes covalently bound to HaloTag protein for  $\text{Na}^+$  imaging. Reprinted with permission from reference [34].

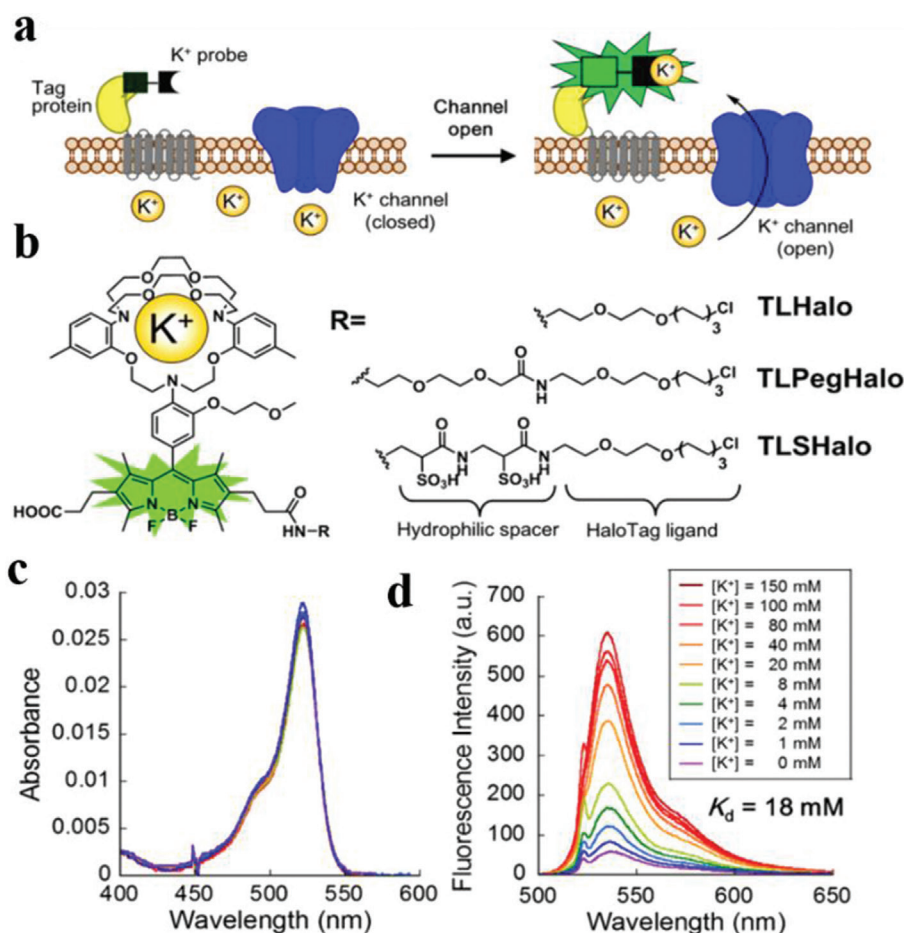
probes show high  $K^+$ -triggered fluorescence enhancement in water samples with physiologically relevant levels of  $K^+$ . A set of highly  $K^+$ -selective fluorescent probes were prepared through varying the lariat-alkoxy unit of a phenylaza-18-crown-6 ionophore to obtain improved  $K^+/Na^+$  selectivity [39]. Among all the probes, an isopropyl group substituted probe showed high  $K^+/Na^+$  selectivity and can serve as a suitable fluorescent probe to measure physiological  $K^+$  levels in the range of 10–80 mM *in vitro*. In addition, a hydrogen-bonded supramolecular framework based on 3,3'-((6-hydroxy-1,3,5-triazine-2,4-diyl) bis(azanediyl))dibenzoic acid and Zn(II) was prepared [40]. The 2D layer architecture is further stacked via hydrogen bond and  $N\cdots N$  van der Waals interactions to form a 3D supramolecular framework. Because of its matched ionic size and charge number,  $K^+$  effectively facilitates the energy transfer process. Apart from the detection of  $K^+$ , the parallel monitoring of  $K^+$  and PPIX in living animals was achieved by a functional nucleic acid (FNA)-based technique [41]. A  $K^+$  induced G-rich FNA probe formed a parallel G-quadruplex with enhanced fluorescence, and thus allowed the detection of  $K^+$  and PPIX. In another case, multi-functional fluorescent probes with high  $K^+$  selectivity were constructed. Using N-(2-methoxyethoxyphenyl) aza-18-crown-6 ionophore, Holdt *et al.*, developed a highly  $K^+$ -selective two-photon fluorescent probe for *in vitro* monitoring of physiological  $K^+$  levels (1–100 mM) [42]. The two-photon excited fluorescence probe shows three times fluorescence enhancement in the presence of 160 mM  $K^+$ . To achieve higher  $K^+$  sensitivity, a fluorescence and resonance Rayleigh scattering (RRS) di-model probe was developed to monitor  $K^+$  coupled N-doped carbon dot (CDUN) and aptamer (Apt) with a detection limit of 0.3 nmol/L [43]. The CDUN encapsulated by Apt reduced its fluorescence and RRS intensities. When  $K^+$  was added, it reacts with Apt to form a stable G-quadruplex and free CDUN. The fluorescence and RRS di-model intensity increased linearly with the concentration of  $K^+$ . Due to its involvement in maintaining membrane potential, monitoring of  $K^+$  around cell membranes is of particular importance. For the first time, a membrane-anchored fluorescent probe for real-time detecting  $K^+$  in the cell microenvironment was reported [44]. This probe exhibits high sensitivity and selectivity to  $K^+$  with a ratiometric fluorescent signal. Especially, the reversible coordination between  $K^+$  and the probe could monitor dynamic changes of  $K^+$  in complex physiological systems. In another study, a protein-coupled fluorescent probe TLSHalo was designed by covalently conjugating the probe with HaloTag protein, which is sensitive to  $K^+$  in the physiological range [45]. The real-time

change of localized extracellular  $K^+$  with TLSHalo was observed under a fluorescence microscope (Figures 2 a–d).

## 2.3 Probes for calcium ions ( $Ca^{2+}$ )

Calcium is the most abundant metal and the fifth-most abundant element in the human body. 99% of the calcium in the body is found in bones and teeth, while the other 1% is found in the blood and soft tissue. As electrolytes, they act as a second messenger in cell-signaling pathways [46,47] where they are involved in mediating the constriction and relaxation of blood vessels (vasoconstriction and vasodilation), nerve impulse transmission, muscle contraction, and the secretion of hormones like insulin. In addition, many enzymes require calcium ions as a cofactor, including several of the coagulation factors. For example, calcium ions are required for the activation of the seven “vitamin K-dependent” clotting factors that control the clotting of blood. For normal physiological functioning, calcium concentrations in the blood and extracellular fluid are tightly controlled by the parathyroid hormone and vitamin D at the expense of the skeleton when dietary calcium intakes are inadequate. The rise or fall of calcium is the molecular clock that times the execution of important processes, therefore, it is crucial to measure  $[Ca^{2+}]$  changes at the cellular level.

A red-emitting BODIPY-based fluorophore was developed for  $Ca^{2+}$  detection [48]. The probe demonstrated good selectivity towards  $Ca^{2+}$  over other metal ions. Upon  $Ca^{2+}$  binding, the probe exhibited 43-fold fluorescence enhancement with the detection limit of 39  $\mu$ M. In another case, a coumarin and pyrazoline derived  $Ca^{2+}$  probe was developed on the basis of PET strategy [49]. The probe could detect  $Ca^{2+}$  rapidly (within 5 s) with a low detection limit ( $2.7 \times 10^{-7}$  M) and can be used for  $Ca^{2+}$  imaging in living A549 cells. Probes with different dyes derived from naphthalene diimide [50], rhodamines, and fluorescein [51,52] enriched the library of  $Ca^{2+}$  sensors and enabled sensitive detection and imaging of biological  $Ca^{2+}$ . Urano *et al.* synthesized silicon-substituted rhodamines with enhanced permeability and far-red emission for  $Ca^{2+}$  imaging in lysosomes and cytosol in living cells and brain [53]. To develop near-infrared (NIR) probe with better bio-compatibility especially *in vivo* applications, Urano *et al.* prepared phosphorus-substituted rhodamines [54]. Results indicated that phosphorus-substituent effectively red shifted the emission of rhodamine to 712 nm, and better sensitivity was achieved compared to

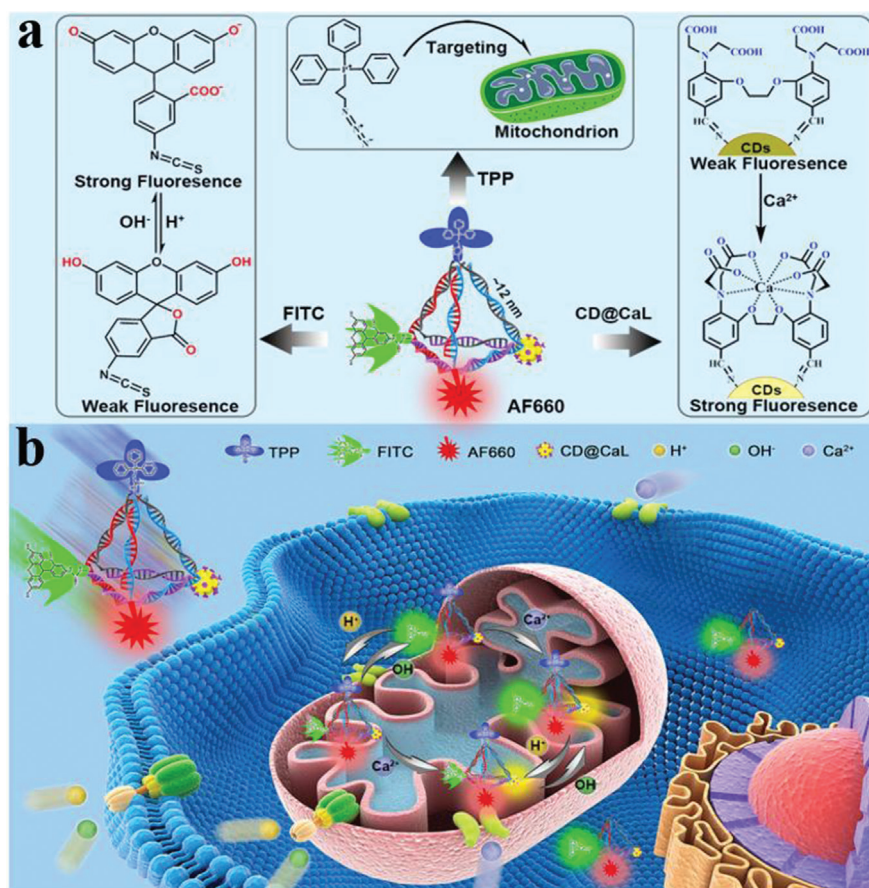


**Figure 2:** (a) Illustration of the probe that detects K<sup>+</sup> channel activity at the cell surface. (b) Chemical structures of the K<sup>+</sup> probes. (c,d) Absorption (c) and emission (d) spectra of TLShalo measured in HEPES buffer containing [K<sup>+</sup>]. Reprinted with permission from reference [45].

that of silicon-substituted rhodamines. The new probe can be also used to image Ca<sup>2+</sup> at dendrites and spines in brain slices, indicating its potential use in neuroscience research. Besides metal ion concentrations, pH values are another important concern in biological systems. The simultaneous quantification of Ca<sup>2+</sup> and pH values can be useful in clinic diagnosis and disease intervention. A Ca<sup>2+</sup> fluorescent probe was assembled onto a DNA nanostructure together with pH-sensitive, mitochondria targeted and inner-reference molecules to carry on dual function (Figure 3a). With this probe in hand, ROS and A $\beta$  triggered transitory cytoplasmic acidosis and activated acid-sensing ion channels in the mitochondrial membrane were observed (Figure 3b) [55,56]. Two-photon fluorescent probe is favorable for *in vivo* applications due to their long absorption wavelength. A Ca<sup>2+</sup> probe was prepared with a two-photon dye and an internal reference dye. The probe could directly and quantify Ca<sup>2+</sup> concentration within live neurons and various tissues including rat spinal cord tissue [57].

## 2.4 Probes for magnesium ions (Mg<sup>2+</sup>)

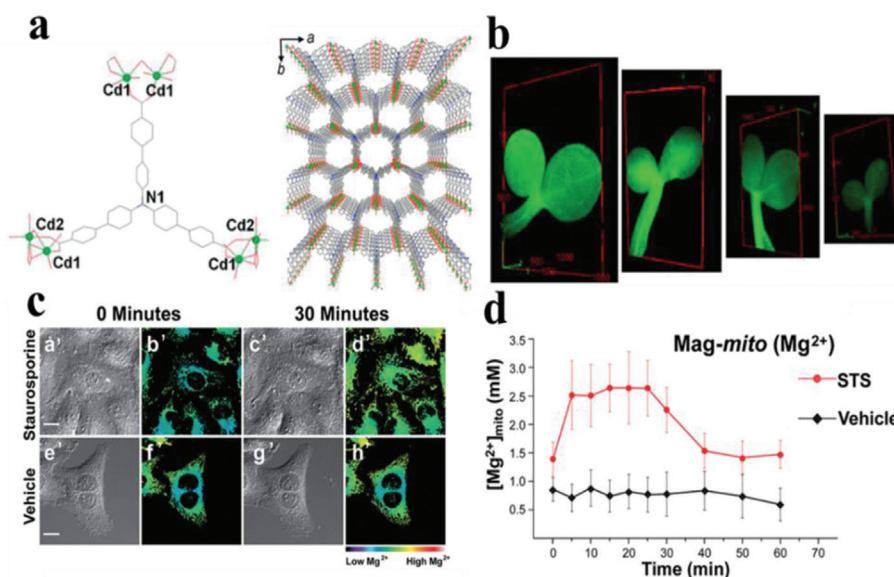
Magnesium is the fourth-most-abundant metal ions in cells (per mole). It is a cofactor in more than 300 enzyme systems that regulate diverse biochemical reactions in our body, including protein synthesis, muscle and nerve function, blood glucose control, and blood pressure regulation [58]. Magnesium is required for energy production, oxidative phosphorylation, and glycolysis. It contributes to the structural development of bone and is required for the synthesis of DNA, RNA, and the antioxidant glutathione. Magnesium also plays a role in the active transport of calcium and potassium ions across cell membranes, a process that is important to nerve impulse conduction, muscle contraction, and normal heart rhythm [59]. However, the understanding of the molecular mechanisms of cellular Mg<sup>2+</sup> homeostasis remains a challenge and demands molecular tools that can detect the ions with high sensitivity. A set of BODIPY-based fluorescence probes was developed for Mg<sup>2+</sup> detection [60].



**Figure 3:** (a) Design of tetrahedron DNA-based  $\text{Ca}^{2+}$  nanoprobe. (b) Mechanism of DNA nanosensor for  $\text{Ca}^{2+}$  and pH sensing. Reprinted with permission from reference [55].

The probes showed 29-fold fluorescence enhancement upon  $\text{Mg}^{2+}$  binding both *in vitro* and in cell, demonstrating high selectivity for  $\text{Mg}^{2+}$ . A natural product, thymol derivatives, were prepared with simple synthetic procedures and used as a fluorescent indicators for  $\text{Mg}^{2+}$  in living cells [61]. Due to the small size and lipophilic character of thymol, the probe exhibits good cell penetration ability that allows the probe to get into subcellular organelles and enables intracellular free  $\text{Mg}^{2+}$  imaging in living RAW 264.7 and HeLa cells. Most fluorescent probes are not reusable. A three-dimensional (3D) MOF with one-dimensional (1D) hexagonal channels was synthesized for  $\text{Mg}^{2+}$  detection (Figure 4a) [62]. This probe can be recycled without signal attenuation. After absorbing  $\text{Mg}^{2+}$ , the fluorescence of MOF increased by 3.2-fold. Furthermore, multi-color imaging [63] and two-photon fluorescent imaging [64] was also used for  $\text{Mg}^{2+}$  detection. Murata et al. developed Si-rhodamine probe with PET-type “off-on” response in the presence of  $\text{Mg}^{2+}$ . In addition, it is possible to visualize the interaction of signals within the cell by using four chromophores for simultaneous multicolor imaging [65]. Two coumarin-based fluorescent probes,

OC7 (methoxy phenyl alkynyl) and NC7 (dimethylamino phenyl alkynyl), were prepared as two-photon fluorophore for  $\text{Mg}^{2+}$  detection [64]. OC7 and NC7 demonstrated significant signals with 9.05-fold and 23.8-fold fluorescence enhancement and large two-photon absorption cross sections (340 and 615 GM) at the NIR wavelengths (740 and 860 nm). Metal ion detection in a specific organelle is often desirable in disease diagnosis [66–68]. A probe with a tetrazine-functionalized pre-sensor and a genetically encoded HaloTag fusion protein conjugate was developed to target a specific cellular localization [65]. The probe was successfully applied for  $\text{Mg}^{2+}$  imaging in different organelles such as the nucleus and Golgi apparatus of HEK 293T cells. A series of fluorescent probes were designed for targeted detection of free  $\text{Mg}^{2+}$  in specific intracellular organelles and their application in the study of programmed cell death were evaluated [66,67]. The triazole-based probe can detect free  $\text{Mg}^{2+}$  levels in mitochondria. Moreover, fluorescence imaging study of Staurosporine-treated HeLa cells directly revealed that the free  $\text{Mg}^{2+}$  levels increase in mitochondria during early apoptosis (Figures 4c,d).

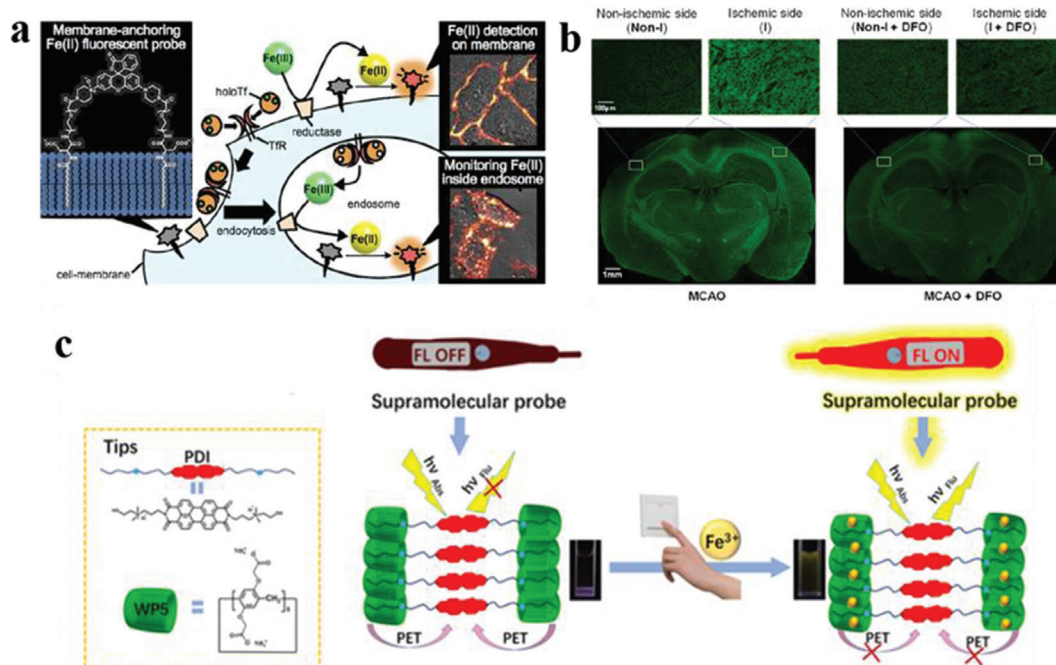


**Figure 4:** (a) Coordination of the ligand to Cd<sup>2+</sup> ions and 3D network structure of 1 with one-dimensional channels along the c axis. Reprinted with permission from reference [62]. (b) 3D fluorescence images of plants with different concentrations of Mg<sup>2+</sup> treatment. Reprinted with permission from reference [68]. (c) Widefield fluorescence imaging of mitochondrial free Mg<sup>2+</sup> in HeLa cells treated with 1 mM apoptosis-inducing Staurosporine (a'-d'), or vehicle (e'-h') and (d) corresponding quantified changes. Reprinted with permission from reference [67].

## 2.5 Probes for iron ions (Fe<sup>2+</sup> and Fe<sup>3+</sup>)

In the human body, iron is the most abundant transition metal. It exists in two biologically relevant oxidation states: the ferrous form (Fe<sup>2+</sup>) and the ferric form (Fe<sup>3+</sup>). Iron plays an essential role in many biological processes [69], such as oxygen transport, energy production, DNA synthesis, and cell growth and replication through iron-dependent proteins. For example, Globin-heme proteins such as hemoglobin, myoglobin, and neuroglobin are involved in oxygen transport and storage. Heme enzymes (e.g. cytochromes a, b, f oxidase) are involved in electron transfer and/or with oxidase activity. Iron-sulfur (Fe-S) cluster proteins are involved in energy production, DNA synthesis or DNA replication and repair. Nonheme enzymes such as phenylalanine and lysine hydroxylases require iron as a cofactor for their catalytic activities. Nonheme proteins such as ferritin and transferrin are responsible for iron transport and storage [70]. In addition to iron-dependent proteins, iron also exists in 'transit labile iron pools' where iron is loosely bound to low molecular-weight compounds such as phosphate, carbonate and citrate. Labile iron ions are toxic to cells, as they promote the production of ROS, which is associated with the aging process and a few degenerative diseases [71]. In addition, the 'transit' iron pool contributes to the cellular iron uptake via transferrin. In order to gain better understanding of the intracellular iron transport mechanisms and the biological

functions of labile irons, effective tools to monitor iron ions in living cells are required. In the past decades, many efforts have been made to develop iron sensors with redox state selectivity, sensitivity, and organelle specificity. An "off-on" Fe<sup>2+</sup> selective fluorescent probe was constructed by incorporating an Fe<sup>2+</sup>-induced N-O cleavage of acylated hydroxylamine moiety into the naphthalimide fluorophore (Figure 5b) [72]. It was demonstrated that the probe can be used to detect endogenous, basal level of labile Fe<sup>2+</sup> pools in living cells and Fe<sup>2+</sup> involved in biological processes, such as the Zn<sup>2+</sup>-induced Fe<sup>2+</sup> flux and the elevated level of Fe<sup>2+</sup> in the brain tissue of a rat undergoing ischemic stroke at the ischemic site. Ion sensors targeting specific cellular localization have emerged in recent years. A Mem-RhoNox probe was developed to monitor local Fe<sup>2+</sup> at the surface of the plasma membrane of living cells [73]. The probe consists of the N-oxygenated rhodamine scaffold with two arms, both of which are tethered with palmitoyl groups as membrane-anchoring domains (Figure 5a). With a model compound Ac-RhoNox in an aqueous buffer, the probe shows a fluorescence turn-on response to the Fe<sup>2+</sup> redox state-selectively and the capability of monitoring endosomal Fe<sup>2+</sup> in primary cultured neurons during endocytotic uptake. To specifically target endogenous mitochondrial Fe<sup>2+</sup> in living cells, a fluorescent probe MtFluNox/Ac-MtFluNox was developed [74]. The deacetylated form, MtFluNox, showed a turn-on response towards Fe<sup>2+</sup> with high metal selectivity in cuvette



**Figure 5:** (a) Schematic illustration of  $\text{Fe}^{2+}$  ions release imaging during endocytotic uptake process. Reprinted with permission from reference [73]. (b) Fluorescent images of labile  $\text{Fe}^{2+}$  in rat's ischemic brain tissue. Reprinted with permission from reference [72]. (c) supramolecular system for  $\text{Fe}^{3+}$  ions sensing. Reprinted with permission from reference [86].

experiments, and an imaging study using its cell-compatible analogue, Ac-MtFluNox, demonstrated mitochondria-specific fluorescence enhancement in response to  $\text{Fe}^{2+}$  in living cells. They also demonstrated that the probe was able to detect endogenously accumulated  $\text{Fe}^{2+}$  induced as a result of the inhibition of heme synthesis. In addition, an organic-inorganic hybrid is reported for ratiometric fluorescent biosensing of  $\text{Fe}^{2+}$  [75]. The probe contained nanoclusters (AuNCs) with a ligand that recognized  $\text{Fe}^{2+}$  and a reference element comprised of water-soluble sulfocyanine 7 Nhydroxysuccinimide ester (Cy7 NHS ester). The fluorescent nanosensor showed great selectivity and accuracy with a detection limit of 210 nM, as well as quick response (detecting time of less than 1.23 s) and long-term stability. Specifically, it displayed good linearity with the concentration of  $\text{Fe}^{2+}$  in the range of  $1\text{--}10^5 \mu\text{M}$ . Furthermore, this probe was successfully applied in real-time biosensing and bioimaging of  $\text{Fe}^{2+}$  in neurons and HepG2 cells. Moreover, a two-photon fluorescence probe for  $\text{Fe}^{2+}$ , DCM-Fe was developed [76]. The probe incorporated dicyanomethylene-4H-pyran (DCM) and a  $\text{Fe}^{2+}$  reduction group (N-oxide) for  $\text{Fe}^{2+}$  sensing. The probe was considered as a “naked-eye colorimetric sensor” as the NIR fluorescence emission ( $\lambda_{\text{em}} = 690 \text{ nm}$ ) increased remarkably with ICT enhanced when the N-oxide is reduced by  $\text{Fe}^{2+}$ . Similarly, a naphthoquinone-based chemosensor was synthesized and applied in human cancer cells and zebrafish [77]. The

probe also featured the ability to sense  $\text{Fe}^{2+}$  via naked-eye detection. The sensing property was evaluated and the detection limit of the ligand 2HPN to  $\text{Fe}^{2+}$  was calculated to be  $0.272 \mu\text{M}$  in aqueous acetonitrile medium by a fluorescence emission method. Another  $\text{Fe}^{2+}$  sensor, Phen-MDI-CA with naked-eye detection mode, was synthesized via chemically bonding 1,10-phenanthroline-5-amine (Phen) onto cellulose acetate (CA) [78]. The sensor displayed excellent fluorescence properties in both solution and solid state. Due to the good solubility and easy processing of Phen-MDI-CA in common organic solvents, it can be used in different material forms. In addition to its fluorescence detection mode, the probe can work in instrument-free visual mode because a red, insoluble, and nonfluorescent Fe-(Phen-MDI-CA) complex appears immediately upon binding to  $\text{Fe}^{2+}$  ions. Recently, great progress has been made in the development of iron probes suitable for *in vivo* application. A live cell-specific probe Racy was reported [79]. The probe was equipped with an acetate group as a switch and showed a highly sensitive and selective response to  $\text{Fe}^{2+}$  ions in the presence of esterase in live cells. The probe was also used to evaluate the esterase activity in live animals. A fluorescent probe DCI-Fe(II) based on the N-oxide chemistry was prepared for real-time detection and imaging of  $\text{Fe}^{2+}$  both in cells and *in vivo* [80]. The probe showed  $\text{Fe}^{2+}$  concentration-dependent NIR fluorescence turn-on response at 700 nm with a

desirably large Stokes shift and a rapid response (5 min) and detection limit of 51 nM for  $\text{Fe}^{2+}$ . In this study, the probe was successfully applied to visualize  $\text{Fe}^{2+}$  in lipid droplets of living cells and living animals.

For the detection and imaging of  $\text{Fe}^{3+}$ , molecular and supramolecular probes, and even 2D/3D materials are prepared as sensors. As a group of molecular probes, rhodamine based dyes were widely used in  $\text{Fe}^{3+}$  sensors. For example, a rhodamine-phenanthroline dye based fluorescent probe was prepared and used to selectively visualize endogenous  $\text{Fe}^{3+}$  levels under stress conditions [81]. The probe can also be used for real time imaging of endogenous  $\text{Fe}^{3+}$  in living C6 cell lines. In another study, a rhodamine-B armed fluorescent chemosensor was designed and synthesized via condensation reaction between rhodamine B hydrazide and naphthyl as a probe for  $\text{Fe}^{3+}$  detection [82]. The probe showed selective turn-on fluorescent change for  $\text{Fe}^{3+}$  over other cations even in the presence of competing trivalent metal ions and gave a detection limit of 0.16  $\mu\text{M}$ . This probe was applied to monitor and image  $\text{Fe}^{3+}$  ions in HeLa cell line and zebrafish. Another Rhodamine B-based fluorescent chemosensor (RBTM) for  $\text{Fe}^{3+}$  was designed [83]. Upon addition of  $\text{Fe}^{3+}$  in aqueous ethanol, the probe displayed significant fluorescence enhancement and distinct color change. The detection limit was calculated to be 0.256  $\mu\text{M}$ . It was also showed that RBTM probe can be used to detect  $\text{Fe}^{3+}$  in MKN-45 cells and dorsal root ganglia. In addition, a rhodamine 6G derivative fluorescent probe named RG5NC was designed [84]. The probe showed high selectivity with a detection limit of 8.2 nM towards  $\text{Fe}^{3+}$  in the presence of various other metal ions and exhibited negligible cytotoxicity in human blood samples and cells. An “off-on” colorimetric and fluorescent probe for  $\text{Fe}^{3+}$  was designed and synthesized [85]. The probe could sensitively respond to  $\text{Fe}^{3+}$  among other tested metal cations in THF- $\text{H}_2\text{O}$  solution with a calculated detection limit of 0.0231  $\mu\text{M}$ . The fluorescence intensity of the probe showed a good linearity with the concentration of  $\text{Fe}^{3+}$  in the range of 0.1 to 26  $\mu\text{M}$ . It was shown that the probe can be used to monitor  $\text{Fe}^{3+}$  level in human blood serum and water samples, and for fluorescence imaging of  $\text{Fe}^{3+}$  in living cell. Supramolecular systems present another promising system for metal ion sensors. Recently, a supramolecular host-guest system ( $\text{WP5} \supset \text{G}$ ) comprised of water-soluble pillar[5]arene (WP5) and quaternized perylene diimide derivative (G) showed great potential as a “turn-on” fluorescent probe (Figure 5c) with a detection limit of 0.213  $\mu\text{M}$  for  $\text{Fe}^{3+}$  ions [86]. 2D material can also be used for ions sensing. For example, Wang et al. demonstrated that two

porous organic polymer nanotubes (PNT-2 and PNT-3) could both serve as luminescent probes for  $\text{Fe}^{3+}$  due to the distinct luminescent quenching upon addition of  $\text{Fe}^{3+}$ , while the luminescent intensities of PNTs have no obvious change after adding other metal ions [87]. Fluorescent  $\text{Ti}_3\text{C}_2$  MXene quantum dots (MQDs) of the size of 1.75 nm were synthesized and used for  $\text{Fe}^{3+}$  detection since the fluorescence of the MQDs can be significantly suppressed by  $\text{Fe}^{3+}$  due to the oxidation–reduction reaction between the MQDs and  $\text{Fe}^{3+}$  and the IFE [88]. The sensor showed high sensitivity with a detection limit of 310 nM and was successfully used to detect  $\text{Fe}^{3+}$  in serum and sea water. Furthermore, a study by Cui et al. described the first example of a 3D MOF-based turn-on  $\text{Fe}^{3+}$  sensor, ZJU-109 [89]. The sensor contained Co as the metal center and 6-(4-pyridyl)-terephthalic acid ( $\text{H}_2\text{pta}$ ) and 4,40-bis(imidazolyl)-biphenyl (4,40-bimbp) as double linkers, a detection limit of 0.053  $\mu\text{M}$  was reported. In addition, another MOF-based potential sensor for  $\text{Fe}^{3+}$  ions was reported by Chang et al. [90]. In this study a channel-type fluorescent Eu (III)-containing metal-organic framework (MOF)  $\{[\text{Eu}_2\text{L}_2] \cdot 2\text{NH}_2(\text{CH}_3)_2\text{DMA}\}$  with a flexible tetracarboxylic acid ligand was successfully prepared. The sensor operated based on a luminescence quenching effect and gave a detection limit of 23  $\mu\text{M}$  in a water solution. In addition, it can be used to treat PD rats, presenting its potential as a candidate for PD treatment.

## 2.6 Probes for zinc ions ( $\text{Zn}^{2+}$ )

Zinc is the second most abundant trace metal in humans after iron, and it plays important roles in growth and development, immune function, neurotransmission, vision, reproduction, and intestinal ion transport [91]. Zinc is the only metal ion that appears in all six enzyme classes and over 300 enzymes [92] and 1000 transcription factors require zinc for their function [93]. In addition, zinc serves a structural role in many proteins. For example, zinc finger motifs in the structure of nuclear receptors allow them to bind to DNA and act as transcription factors to regulate gene expression. Zinc has been found to influence hormone release [94] and nerve impulse transmission [95]. Dietary zinc deficiency has been associated with impaired growth and development in children, pregnancy complications, and immune dysfunction with increased susceptibility to infections [96]. Due to the importance of  $\text{Zn}^{2+}$  in biology and the growing evidence that  $\text{Zn}^{2+}$  levels are both heterogeneous and dynamic,  $\text{Zn}^{2+}$  attracted the most attention regarding the development of fluorescent sensors for

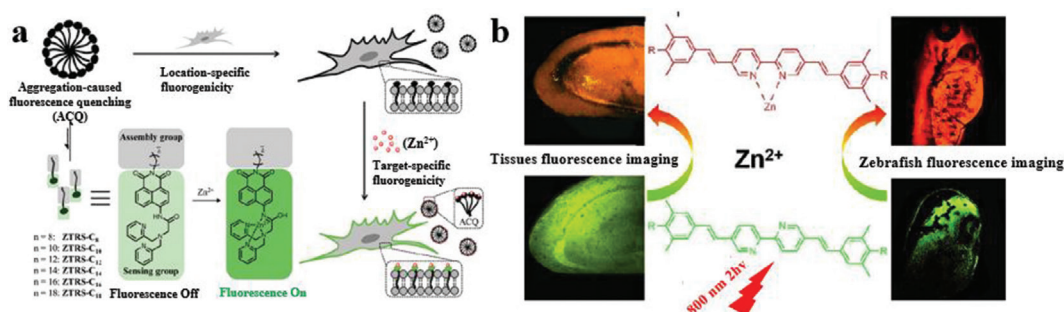
transition metals. Recently, a reversible fluorescence  $\text{Zn}^{2+}$  sensor [97] based on 8-aminoquioline was reported. The probe showed a remarkable low detection limit (2.15 nM) in aqueous solution. A fluorescein based colorimetric turn-on fluorescent sensor was prepared and applied to detect  $\text{Zn}^{2+}$  in apoptotic HEK 293 cells [98]. This probe can be used as an instrument-free sensor as drastic color changes was observed upon  $\text{Zn}^{2+}$  binding. To minimize the background interference, a NIR fluorescent  $\text{Zn}^{2+}$  probe based on dicyanoisophorone was developed [99]. This probe showed a very large stokes shift ( $\lambda_{\text{em}} - \lambda_{\text{ex}} = 168 \text{ nm}$ ), which provides high contrast for  $\text{Zn}^{2+}$  sensing. A naphthalene imide-based probe was developed for plasma membrane-specific  $\text{Zn}^{2+}$  detection by introducing membrane-anchoring domains of hydrophobic alkyl chains [100]. The probe assembled into aggregates and exhibited ACQ (Figure 6a). When anchoring on the membrane surface that led to the probe disaggregate, the probe exhibited a fluorescence-enhanced response upon recognition of zinc ions. Another novel strategy for detecting  $\text{Zn}^{2+}$  through a so-called multiple steps process was presented [101]. A bis-Schiff base fluorescent probe based on 2-(benzo[d]oxazol-2-yl) phenol was designed and synthesized. The as-prepared probe can be used to monitor  $[\text{Zn}^{2+}]$  levels in a Parkinson's disease model *in vitro* via chelation-hydrolysis interaction. In order to detect  $\text{Zn}^{2+}$  *in vivo* and in tissue, a cyanine-based fluorescent probe was constructed [102]. This probe exhibited a high fluorescence quantum yield upon binding to  $\text{Zn}^{2+}$  and was successfully used to detect endogenous  $\text{Zn}^{2+}$  in living zebrafish. Furthermore, to enhance the sensitivity of  $\text{Zn}^{2+}$  sensor in organisms, a fluorescent probe based on dye-assembled lanthanide-doped upconversion nanoparticles was prepared and used to detect  $\text{Zn}^{2+}$  in mouse brain slice with Alzheimer's disease and zebrafish [103]. This nano system showed a low detection limit (78 nM) and quick response (within 5 s) via blocking the FRET process. To further improve

tissue depth penetration of probes, Okamoto *et al.* reported a two-photon, fluorescent  $\text{Zn}^{2+}$  probe that enables the monitoring of presynaptic  $\text{Zn}^{2+}$  dynamics at the single-synapse level in mossy fiber termini of neurons in adult mice hippocampal tissue [104]. Similarly, a two-photon, fluorescence probe was developed with intramolecular charge transfer, that allows the ratiometric determination of  $\text{Zn}^{2+}$  [105] (Figure 6b). This probe features high temporal resolution and a low detection limit ( $\sim 15 \text{ nM}$ ), and can be used for  $\text{Zn}^{2+}$  detection in hippocampal tissue with Alzheimer's disease and zebrafish.

## 2.7 Probes for copper ions ( $\text{Cu}^{2+}$ )

Copper is essential to all living organisms as a trace dietary mineral. In humans, copper is found mainly in the liver, muscle, and bone [106], and it is necessary for the proper growth, development, and maintenance of bone, connective tissue, brain, heart, and many other body organs. It is involved in the formation of red blood cells, iron metabolism, the metabolism of cholesterol and glucose, and the synthesis and release of life-sustaining proteins and enzymes. These enzymes, in turn, produce cellular energy and regulate nerve transmission, blood clotting, and oxygen transport. Copper also stimulates the immune system to fight infections, to repair injured tissues, and to promote healing [107]. Acquired copper deficiency is linked to symptoms including deficiencies in blood cells, bone and connective tissue abnormalities, and neurologic disorders. Many detection methods of copper have provided valuable information for a better understanding of the complex handling of copper in cells.

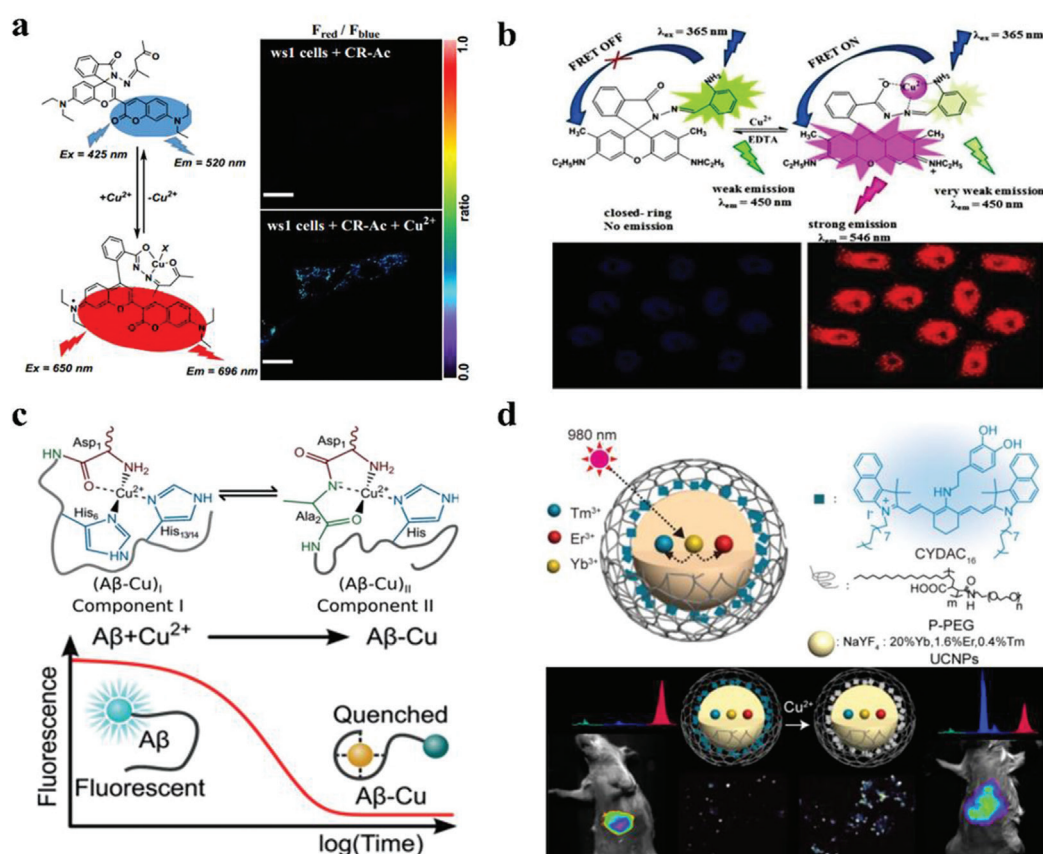
A novel “off-on” fluorescence probe was designed using two rhodamine B moieties [108]. Upon the addition of  $\text{Cu}^{2+}$ , the probe showed almost 40-fold enhancement in fluorescence intensity at 580 nm. The probe



**Figure 6:** (a) Fluorescence probe for imaging  $\text{Zn}^{2+}$  at the surface of the plasma membrane. Reprinted with permission from reference [100]. (b) Two-photon responses of  $\text{Zn}^{2+}$  probe for imaging in brain tissue and zebrafish. Reprinted with permission from reference [105].

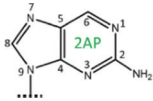
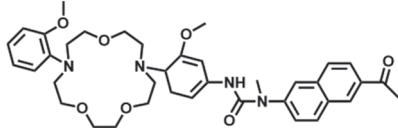
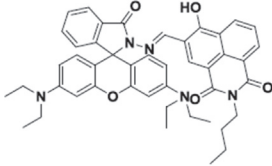
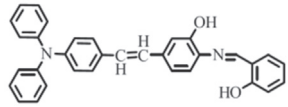
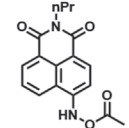
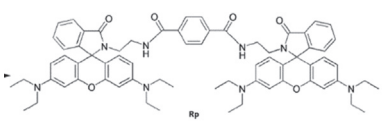
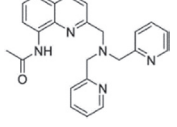
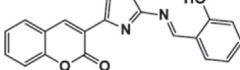
exhibited high selectivity and sensitivity (detection limit is 38 nM) for  $\text{Cu}^{2+}$ . A coumarin-salicylidene Schiff based “on-off” probe was constructed [109]. The probe exhibits fluorescence quenching caused by  $\text{Cu}^{2+}$  through a chelation-enhanced quenching process. The probe showed a lower fluorescence detection limit of 24 nM, and was successfully used to measure  $\text{Cu}^{2+}$  in tap water and pharmaceutical samples. In addition, an ultrasensitive naphthalimide-derived probe was designed and used in living cells [110]. The probe showed fluorescence intensity decrease at 541 nm as the concentration of  $\text{Cu}^{2+}$  increased due to the suppression of ICT process. A new aggregation-induced ratiometric fluorescent probe was prepared for  $\text{Cu}^{2+}$  detection [111]. Upon  $\text{Cu}^{2+}$  binding, the fluorescence of the probe showed a color change due to aggregation and ICT process. The probe was successfully used to detect  $\text{Cu}^{2+}$  in HeLa cells. Most ratiometric probes operate on the FRET mechanism. A FRET-based ratiometric  $\text{Cu}^{2+}$  probe

was synthesized using rhodamine 6G and 2-formylaniline [112]. The binding between the probe and  $\text{Cu}^{2+}$  induced the opening of the spiro-ring, which enabled the FRET process (Figure 7b), resulting in an apparent yellow fluorescence at 546 nm. In another study, a benzimidazole-quinoline based ratiometric probe for  $\text{Cu}^{2+}$  was prepared [113]. The probe showed an obvious red shift (132 nm), which can be visualized by the “naked-eye”. In recent years, many fluorescence probes with high sensitivity, improved biocompatibility and penetrability, have been developed for  $\text{Cu}^{2+}$  detection in living systems (Table 1). For example, a NIR ratiometric fluorescent probe exhibited an obvious fluorescent color change from blue to red upon the addition of  $\text{Cu}^{2+}$ . The fluorescent ratiometric change ( $F_{\text{red}}/F_{\text{blue}}$ ) was analyzed to quantify free  $\text{Cu}^{2+}$  levels in cells [114] (Figure 7a). In addition, the probe showed fast response to  $\text{Cu}^{2+}$  and resisted pH values change, indicating the great potential for studying  $\text{Cu}^{2+}$  in cell biology.



**Figure 7:** (a) NIR ratiometric fluorescent probe for monitoring the dynamic changes of subcellular  $\text{Cu}^{2+}$ . Reprinted with permission from reference [114]. (b)  $\text{Cu}^{2+}$  detection based on FRET mechanism. Reprinted with permission from reference [112]. (c)  $\text{Cu}^{2+}$  coordination to  $\text{A}\beta$  at physiological pH. Reprinted with permission from reference [115]. (d) Dye-upconversion nanocomposite for ratiometric fluorescence Bioimaging of  $\text{Cu}^{2+}$  ions *in vivo*. Reprinted with permission from reference [116].

**Table 1:** Typical fluorescence probes for metal ions

Metal ions	Probes	Detection limit	Fluorescence peak	Reference
Na <sup>+</sup>		0.4 mM	370 nm	[34]
K <sup>+</sup>		160 mM	860 nm	[42]
Ca <sup>2+</sup>		2.7×10 <sup>-7</sup> M	537 nm	[50]
Mg <sup>2+</sup>		1.47×10 <sup>-6</sup> M	590 nm	[68]
Fe <sup>2+</sup>		0.5 μM	544 nm	[80]
Fe <sup>3+</sup>		0.0231 μM	550 nm	[85]
Zn <sup>2+</sup>		2.15 nM	510 nm	[97]
Cu <sup>2+</sup>		24 nM	544 nm	[109]

Cu<sup>2+</sup> was considered as one of the metal ions that promotes Amyloid-β (Aβ) aggregation, which was proposed as a highly relevant factor in Alzheimer's disease. A fluorescent probe consisting of clioquinone and Aβ peptides was used to investigate the kinetics of the interaction between Aβ and Cu<sup>2+</sup> in a physiological environment, as Cu<sup>2+</sup> can cause fluorescent quenching of the probe [115] (Figure 7c). Another NIR probe with cyanine conjugated Lanthanide-doped upconversion nanoparticles (UCNPs) was prepared to detect Cu<sup>2+</sup> in living cells and animal tissues [116] (Figure 7d). It was demonstrated that the UCNPs conjugate decreased detection limit of cyanine probe from 78 to 37 nM. In addition, the probe provided real-time detection that is suitable for biological application.

### 3 Perspective

We briefly reviewed the recent advances in the detection and imaging of metal ions in biological systems using organic dye-based fluorescent sensor. With various modifications, these organic dyes can be used to specifically detect different metal ions in various organisms and cells and provide useful information on the concentration, distribution and even dynamics of metal ions in cells. This information helps us gain insight into biological pathways and metabolic processes, and benefits diseases diagnose. Despite all the progress that has been made in the development of organic dyed based fluorescent probes, several issues

still remain in this field, which has been summarized as follows:

- (1) In addition to their role of static cofactors buried within protein active sites, most transition metal ions are also present in loosely bound, labile pools that can participate in critical biological processes such as signaling pathways. Metal ion homeostasis is tightly regulated by cells and tissues. Disrupting the homeostasis can cause disorders and vice versa. Therefore, developing metal ions sensors that could provide real-time monitoring and reveal the dynamics of metal ions will be desirable.
- (2) Fluorescent probes have been widely used for metal ions detection *in vitro*. However, the *in vivo* applications of fluorescence probes were hampered by the limitation of the penetration depth of the excitation light. Therefore, development of probe with red-shifted absorption, especially in NIR-II region, will be the future direction for fluorescent probe design.
- (3) Despite their advantages, most organic dyes suffer from photobleaching. In addition, the lesion site might have low pH values, high reactive oxygen species or enzyme concentrations. All of these factors will affect the stability of organic dyes. Therefore, improving the stability of organic dyes is another problem to be solved.

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